

1 **Association of strength, power, and function with muscle thickness, echo intensity, and lean**
2 **tissue in older males**

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12

13 **Abstract**

14 **Purpose:** Dual-energy x-ray absorptiometry (DXA) appendicular lean tissue is used to screen
15 older adults for sarcopenia. However, emerging data indicates that ageing-related muscle atrophy
16 largely occurs within specific muscles, which may be masked using appendicular lean tissue.
17 Comparisons between appendicular lean tissue and site-specific measures of muscle in relation to
18 strength and physical function are needed to advance our understanding of these features in the
19 context of poor muscle function in aged adults. Our primary objective was to compare
20 correlations between lean tissue and site-specific muscle characteristics in relation to strength
21 and physical function in older males.

22 **Methods:** Older males (≥ 65 years) were evaluated for muscle strength, physical function (6-
23 minute walk and 30-second sit-to-stand), and muscle size (appendicular and site-specific) and
24 composition (echo intensity) using DXA and ultrasound.

25 **Results:** Of the 32 older males (75.4 ± 7.9 years), 12 had low appendicular lean tissue. All DXA
26 and ultrasound muscle characteristics were associated ($r=0.39$ to 0.83 , $p<0.05$) with torque or
27 power producing capabilities. Except for the knee flexors, no differences in correlation
28 coefficients were observed between muscle thickness or regional lean tissue in relation to muscle
29 strength. Neither DXA nor ultrasound muscle characteristics were associated with physical
30 function.

31 **Conclusions:** In older males, ultrasound-based muscle thickness and DXA lean tissue provided
32 similar associations with strength.

33 **Bullet points:**

- 34
 - Lean tissue and muscle thickness provide similar associations with strength

35 • Muscle thickness can distinguish low and normal appendicular lean tissue in older
36 adults

37 **Keywords:** ultrasound, dual-energy x-ray absorptiometry, sarcopenia, aging

38

39 **Introduction**

40 Sarcopenia is a progressive ageing-related condition that is characterized by impairments
41 in muscle strength, mass, and composition (i.e., increased intramuscular adipose tissue) (Cruz-
42 Jentoft et al. 2018), which is associated with risk of falls and poor physical function (Landi et al.
43 2012). Identification of older adults with sarcopenia is important for providing targeted therapies
44 (e.g., nutritional interventions) to mitigate the progression of this condition. Appendicular lean
45 tissue mass measured using dual-energy x-ray absorptiometry (DXA) is the primary metric for
46 identifying older adults with low muscle mass. While appendicular lean tissue provides surrogate
47 measures of the muscle mass contained within the upper and lower limbs (Chen et al. 2007), we,
48 and others, have observed that compared with younger adults, older adults display smaller
49 muscle thickness for the rectus abdominis (~30-35% smaller) and quadriceps (~25-30% smaller)
50 muscles in comparison to several other limb muscle groups (Abe et al. 2014a, 2014c; Ata et al.
51 2019; Kara et al. 2020; Paris et al. 2020, 2021). Focusing ageing-related assessments of skeletal
52 muscle tissue to those muscle groups that present with earlier and significant declines may
53 provide more sensitive markers for characterizing the progression of muscle atrophy. However,
54 these muscle group specific measures of muscle size (and composition) have not been compared
55 with DXA appendicular lean tissue mass in the context of strength, power, and physical function
56 in older adults. A more thorough comparison of DXA lean tissue and site-specific measures of
57 skeletal muscle size and composition in relation to strength and functional capacity of older
58 adults will assist with developing protocols for identification of older adults with sarcopenia.

59 Ultrasound has emerged as a portable, non-invasive, and cost-effective tool to quantify
60 site-specific muscle mass and composition (Paris and Mourtzakis 2016; Mourtzakis et al. 2017).
61 Ultrasound-measured muscle thickness is strongly associated with volume and whole-body

62 indices of muscle mass measured using reference methods such as magnetic resonance imaging
63 (Sanada et al. 2006) and DXA (Takai et al. 2014; Paris et al. 2017). Muscle echo intensity, a
64 surrogate ultrasound-based measure of muscle composition, is associated with increased
65 intramuscular adipose and connective tissue infiltration (Young et al. 2015; Akima et al. 2016;
66 Stock and Thompson 2020) and increases with advancing age for several muscle groups across
67 the body (Fukumoto et al. 2015; Paris et al. 2020). Therefore, ultrasound represents a promising
68 tool to assess site-specific muscle mass and composition in the progression of sarcopenia.

69 The primary objective of this study was to compare the correlation coefficients between
70 skeletal muscle function and characteristics of skeletal muscle tissue derived using ultrasound
71 (thickness and echo intensity) or DXA (appendicular and regional lean tissue) in a cohort of
72 older males. Skeletal muscle function included evaluation of upper and lower body isometric
73 torque and isokinetic power, and physical function (e.g., 30-second sit to stand). As a secondary
74 objective, we compared lean tissue, muscle thickness, echo intensity, and muscle function
75 between older males with normal versus low appendicular lean tissue mass.

76 **Methods**

77 Study design and participants

78 We recruited 32 community dwelling older (≥ 65 years old) males to attend 2 data
79 collection sessions over of the course of 7-14 days, which included analysis of body
80 composition, physical function, and muscle strength. Recruitment was limited to males due to the
81 necessity for sex-specific analyses (e.g., muscle strength) and the larger age-related impairments
82 in skeletal muscle mass in males with advancing age (Paris et al. 2020). Participants were
83 excluded if they had: 1) a neuromuscular disorder, 2) oral or intra-venous contrast within the past

84 3 weeks, 3) a prosthetic joint replacement, 4) a history of cancer or cerebrovascular disease, or 5)
85 participated in structured exercise sessions within the past 6 months. Prior to all laboratory visits,
86 participants were instructed to refrain from moderate to vigorous physical activity for 48 hours
87 and alcohol consumption for 24 hours. This study was approved by a human research ethics
88 committee at the University of Waterloo. Written informed consent was obtained from all
89 participants in accordance with established protocols for human research.

90 Anthropometry

91 Participant's height and body mass were obtained while wearing a cloth hospital gown
92 using a stadiometer (to the nearest 0.1 cm) and balance beam scale (to the nearest 0.1 kg),
93 respectively. Waist circumference was measured to the nearest 0.1 cm by placing the inferior
94 border of a flexible tape measure at the top of the iliac crest.

95 Ultrasound landmarking

96 Landmarking was performed on participants in a supine or prone posture on a table, with
97 their feet secured in neutral rotation using a foot strap. The upper arm was imaged on the anterior
98 and posterior surface, 60% distal from the acromial process to the lateral epicondyle of the
99 humerus. Anterior forearm images were captured on the anterior surface, 30% distal from the
100 radial head to the styloid process of the radius. Anterior abdomen images were taken 3 cm right
101 of the umbilicus. Anterior thigh images were taken two-thirds the distance from the anterior
102 superior iliac spine to the superior pole of the patella. The posterior upper leg image was taken
103 50% the distance between the greater trochanter and lateral epicondyle of the femur, on the
104 posterior surface. The anterior and posterior lower leg images were taken 30% distal from the
105 head of the fibula to the lateral malleolus. During landmarking, participants remained supine or

106 prone for 20 minutes prior to image acquisition to mitigate shifts in fluid distribution (Berg et al.
107 1993).

108 Ultrasound image acquisition

109 Images were taken in the transverse plane using a real time B-mode ultrasound imaging
110 device (M-turbo, Sonosite, Markham, ON), which was equipped with a multi-frequency linear
111 array transducer (L38xi: 5-10 MHz). Adjustable parameters gain, time-gain-compensation, and
112 dynamic range (50%) were held constant throughout acquisition. To minimize tissue
113 compression during imaging, the ultrasound transducer was generously coated with water-
114 soluble transmission gel, as previously described (Paris et al. 2017). Medial-lateral movement of
115 the transducer was allowed for all landmarks to centre the muscle within the field of view. All
116 landmarks were imaged twice.

117 Muscle thickness and echo intensity

118 Muscle thickness was analyzed for each landmark by measuring the vertical distance
119 between the upper margin of either the underlying bone or the deep muscle fascia (anterior
120 abdomen and anterior lower leg) and the superior muscle fascia. Muscle echo intensity was
121 evaluated by selecting the largest rectangular area within the muscle fascia borders, as previously
122 described (Caresio et al. 2014). Specific muscles analyzed were the rectus abdominis (anterior
123 abdomen), tibialis anterior (anterior lower leg), biceps brachii (anterior upper arm), rectus
124 femoris (anterior upper leg), lateral gastrocnemius (posterior lower leg), and triceps brachii
125 (posterior upper arm). Muscle thickness and echo intensity were measured once per image (two
126 images per landmark) by a single trained investigator and averaged for each landmark (Figure 1).
127 Ultrasound measures of muscle thickness and echo intensity have been previously demonstrated

128 to be a reliable technique in older adults for several muscle groups (Strasser et al. 2013; Nijholt
129 et al. 2017) Muscle thickness and echo intensity measurements were performed using ImageJ
130 (NIH, Bethesda, MD, version 1.53e) by a single trained investigator.

131 Dual-energy x-ray absorptiometry

132 A certified medical radiation technologist performed all whole body DXA scans (Hologic
133 discovery QDR4500, Hologic, Toronto, ON). Hologic software (version 13.2) was used to
134 segment the body into the head, torso, left and right arms, and left and right legs. Appendicular
135 lean tissue index was calculated by dividing the sum of the lean soft tissue (i.e., fat- and bone-
136 free mass) in the arms and legs by height squared (kg/m^2). Participants were classified as low
137 appendicular lean tissue if they were $<7.0 \text{ kg}/\text{m}^2$ (Cruz-Jentoft et al. 2018). Custom region of
138 interest boxes were placed around: 1) the lower arm, horizontally across the medical epicondyle
139 of the humerus, and 2) the lower leg, horizontally across the tibial plateau. Upper arm and upper
140 leg lean tissue was calculated by subtracting the lower arm or leg lean tissue from the total arm
141 or leg lean tissue, respectively.

142 Isometric torque and isokinetic power

143 All participants performed 1 familiarization session for maximal isometric torque and
144 isokinetic power prior to the testing session, which has been shown improve maximal muscle
145 activation of older adults for strength assessment (Jakobi and Rice 2002). An isokinetic
146 dynamometer (Biodex System 3, Biodex Medical Systems, New York) was used to assess the
147 peak isometric torque of the knee and elbow flexors and extensors and peak isokinetic power of
148 the knee extensors. Participants were seated against the backrest with a hip angle of 85° and
149 straps placed tightly across the participant's waist and chest.

150 Maximal voluntary isometric torque of the elbow extensors and flexors was performed at
151 90° of flexion (confirmed using a goniometer). Alternating between flexion and extension, 6
152 contractions (each lasting 5 seconds) were performed with 30 seconds of rest between trials.
153 Maximal voluntary isometric torque of the knee extensors and flexors was performed at 60° of
154 flexion. Alternating between flexion and extension, 6 contractions (each lasting 5 seconds) were
155 performed with 30 seconds of rest between trials. Maximal voluntary isokinetic power for the
156 knee extensors was evaluated for 3 contractions at 1.05 rad/s (60°/s) and 3 contractions at 3.14
157 rad/s (180°/s), with one minute of rest between trials. For isokinetic power, participants began
158 with their knee at 90° and extended as rapidly and forcefully as possible until 30° deg of flexion.
159 The highest value for maximal torque or peak power across all trials was used for further
160 analysis.

161 Handgrip strength

162 Grip strength of the right hand was assessed using a Jamar hand-held dynamometer
163 according to a standardized protocol (Roberts et al. 2011). Briefly, participants were seated
164 upright in a chair with their right arm placed on the armrest and their elbow flexed to 90°.
165 Participants squeezed with as much force as possible for 3 seconds. Three trials were performed
166 with 1 minute of rest between contractions.

167 Physical function

168 The six-minute walk test was performed using two cones placed 20 m apart. Participants
169 were instructed complete as many “laps” as possible between the cones within 6 minutes
170 (without running or jogging) according to a standardized protocol (Crapo et al. 2002). A 30-
171 second sit-to-stand test was performed with participants’ arms crossed over the chest to prevent

172 assistance during standing. Participants were instructed to fully stand up and sit down as many
173 times as possible within 30 seconds. The chair's seated surface was approximately 46 cm from
174 the ground.

175 Statistical analysis

176 Differences between older adults presenting with low or normal appendicular lean tissue
177 were evaluated using independent sample t-tests. Due to differences in sample size between
178 groups, Hedges' g was used to compute effect sizes and 95% confidence intervals (CI). Pearson
179 correlation coefficients were used to evaluate associations between skeletal muscle
180 characteristics (muscle thickness, echo intensity, or lean tissue mass) and isometric torque,
181 isokinetic power, or physical function. To examine if correlation coefficients were different
182 between muscle thickness or regional lean tissue mass in relation to isometric torque or
183 isokinetic power, a Pearson and Filon's z was used within the cocor software package
184 (Diedenhofen and Musch 2015). Sample size estimates (n=32) were based on expected
185 correlation coefficients between muscle size (thickness, lean tissue, and metrics of strength and
186 power (expected $r=0.35$). Multiple linear regression was used to evaluate the combined effects of
187 muscle thickness and echo intensity on associations with isometric torque or isokinetic power.

188 Statistical significance was set as $p<0.05$. To correct for multiple comparisons between
189 older adults with low vs. normal appendicular lean tissue index, a Holm-Bonferroni correction
190 was used to maintain a family wise error rate of 0.05 for torque and power (n=9), muscle
191 thickness (n=8), and echo intensity (n=6), independently. Similarly, to correct for multiple
192 correlation coefficients, a Holm-Bonferroni correction was used to maintain a family wise error
193 rate of 0.05 for isokinetic torque or power (n=26) and physical function (n=16). All statistical
194 analyses were performed using SPSS (version 26, IBM, USA), unless previously noted.

195 **Results**

196 Males classified as low appendicular lean tissue (n=12) were older ($p<0.001$) and had a
197 lower body mass index (BMI) ($p=0.004$) compared with those with normal appendicular lean
198 tissue (n=20) (Table 1). Compared with the normal appendicular lean tissue group, the low
199 appendicular lean tissue group had lower maximal isometric torque of the knee extensors
200 ($p=0.048$), knee flexors ($p=0.009$), and elbow flexors ($p=0.008$) and peak isokinetic power for
201 knee extensors at 60 °/s ($p=0.049$) (Table 2).

202 Muscle thickness for all evaluated landmarks was smaller ($p<0.05$) in the low compared
203 with normal appendicular lean tissue group, except for the anterior lower leg ($p<0.05$), which
204 was larger in the low appendicular lean tissue group (Table 3). All muscle thicknesses were
205 significantly associated with appendicular and corresponding limb lean tissue mass
206 (Supplementary Table S1). The low appendicular lean tissue group displayed higher echo
207 intensity of the anterior upper leg ($p=0.003$) and anterior lower leg ($p=0.016$) compared to the
208 normal appendicular lean tissue group (Table 4).

209 Maximal isometric torque of the knee extensors was significantly associated with anterior
210 upper leg muscle thickness ($r=0.50$, $p=0.023$) and echo intensity ($r=-0.41$, $p=0.038$) and
211 appendicular ($r=0.52$, $p=0.017$) and upper leg ($r=0.70$, $p<0.001$) lean tissue (Table 5). Peak
212 isokinetic power of the knee extensors at 60 and 180 °/s were significantly associated with
213 anterior upper leg muscle thickness ($r=0.55$, $p=0.010$; $r=0.62$, $p=0.002$) and echo intensity ($r=-$
214 0.47 , $p=0.025$; $r=-0.48$, $p=0.028$) and appendicular ($r=0.57$, $p=0.007$; $r=0.57$, $p=0.007$) and upper
215 leg ($r=0.71$, $p<0.001$; $r=0.63$, $p=0.002$) lean tissue. Maximal isometric torque of the knee flexors
216 was significantly associated with the posterior upper leg muscle thickness ($r=0.39$, $p=0.025$) and
217 appendicular ($r=0.69$, $p<0.001$) and upper leg ($r=0.71$, $p<0.001$) lean tissue (Table 5).

218 Maximal grip strength was significantly associated with anterior forearm thickness
219 ($r=0.53$, $p=0.015$) and appendicular ($r=0.63$, $p=0.002$) and lower arm ($r=0.65$, $p=0.001$) lean
220 tissue (Table 5). Maximal isometric torque of the elbow extensors was significantly associated
221 with posterior upper arm muscle thickness ($r=0.71$, $p<0.001$) and echo intensity ($r=-0.59$,
222 $p=0.005$) and appendicular ($r=0.66$, $p<0.001$) and upper arm ($r=0.83$, $p<0.001$) lean tissue.
223 Maximal isometric torque of the elbow flexors was significantly associated with anterior upper
224 arm muscle thickness ($r=0.58$, $p=0.006$) and echo intensity ($r=-0.43$, $p=0.040$) and appendicular
225 ($r=0.58$, $p=0.006$) and upper arm ($r=0.65$, $p=0.001$) lean tissue (Table 5). Apart from maximal
226 isometric torque of the knee flexors ($p=0.010$), no differences were observed ($p>0.05$) for the
227 correlation coefficients between ultrasound muscle thickness or DXA regional lean tissue in
228 relation to isometric torque or isokinetic power (Table 5).

229 Significant correlations were observed between muscle thickness and echo intensity for
230 the anterior upper arm ($r= -0.47$, $p=0.007$), posterior upper arm ($r= -0.63$, $p=0.001$), and anterior
231 upper leg ($r= -0.66$, $p<0.001$). In a multiple linear regression of muscle thickness and echo
232 intensity, muscle thickness for the anterior upper leg and anterior and posterior upper arm
233 ($p<0.05$), but not echo intensity ($p>0.05$), were significantly associated with their corresponding
234 torque or power, except for the anterior upper leg muscle thickness and isometric torque ($p=0.06$)
235 (Table 6).

236 After correction for multiple comparisons, muscle thickness, echo intensity, appendicular
237 lean tissue, and lower body lean tissue were not associated ($p>0.05$) with six-minute walk or 30-
238 second sit to stand tests (Table 7).

239 **Discussion**

240 Here, we demonstrated that DXA lean tissue (appendicular and regional) and ultrasound
241 site-specific muscle thickness provide similar correlation coefficients with static and dynamic
242 muscle strength in older males. However, upper leg lean tissue mass provided a stronger
243 association with isometric knee flexor torque than the posterior upper leg muscle thickness.
244 While both muscle thickness and echo intensity were correlated with isometric torque and
245 isokinetic power, echo intensity was not independently associated with muscle strength when
246 combined with muscle thickness using multiple linear regression. Compared with older males
247 who had normal appendicular lean tissue mass, all muscle thicknesses were thinner and muscle
248 echo intensity of the rectus femoris and tibialis anterior were greater in the low appendicular lean
249 tissue group.

250 Ageing-related losses in skeletal muscle mass and function are thought to begin around
251 the 5th decade of life and accelerate with advancing age (Mitchell et al. 2012). Even amongst
252 apparently healthy, community dwelling older adults, these ageing-related impairments in
253 muscle tissue progress at a subclinical level; however, there is significant variability in the
254 severity and rate of progression of sarcopenia between individuals (Larsson et al. 2019). Due to
255 this significant variability and the deleterious impact on mobility, independence, health care
256 costs, and rates of mortality, operationalizing a definition of sarcopenia is prudent to enable
257 identification of older adults who may require targeted therapies to mitigate further deterioration
258 (Prado and Heymsfield 2014).

259 DXA measured appendicular lean tissue mass is typically suggested as the primary metric
260 to evaluate ageing-related changes in muscle mass (Cruz-Jentoft et al. 2018). However, as we
261 and others have previously shown, aging is associated with more prominent atrophy of specific

262 muscle groups, such as the rectus abdominis and quadriceps (Abe et al. 2011; Paris et al. 2020,
263 2021). Yet, it remains unclear whether site-specific skeletal muscle atrophy differs in individuals
264 with low vs. appendicular lean tissue mass. Here, we observed that older males with low
265 appendicular lean tissue mass presented with smaller muscle thickness (~13-23%) across all sites
266 except for the anterior lower leg (~8.5%), which was larger. These increases in the anterior lower
267 leg muscle thickness may be related to increased intramuscular adipose tissue or disturbances in
268 fluid balance, as we also observed increased echo intensity of the tibialis anterior muscle in the
269 low compared to normal appendicular lean tissue group. Several other publications have also
270 observed smaller muscle thicknesses for the biceps (~10%), quadriceps (~15-25%), and
271 gastrocnemius muscles (~15-20%) amongst frail (Akazawa et al. 2016), pre-sarcopenic (Minoru
272 et al. 2017), sarcopenic (Kuyumcu et al. 2016; Minoru et al. 2017), functionally-dependent
273 (Akazawa et al. 2016), and weak (Minoru et al. 2017; Chang et al. 2018) older males and
274 females when compared to older adults with normal muscle mass or strength. Increased muscle
275 echo intensity (~17%) has also been observed in the quadriceps (Akazawa et al. 2016; Minoru et
276 al. 2017), but not the biceps (Chang et al. 2018) or gastrocnemius (Chang et al. 2018) muscles in
277 these same cohorts of older adults, which is in agreement with our observations. Taken together,
278 these data suggest that typical ageing-related atrophy may occur in specific muscle groups (e.g.,
279 quadriceps); however, the progression towards a reduced capacity (e.g., low muscle mass) may
280 involve more global muscle atrophy. Therefore, appendicular lean tissue may be a useful index
281 for identification of those older adults with progressed losses in muscle mass, whereas regional
282 or site-specific measures may be more sensitive to early ageing-related losses.

283 In relation to isometric torque or isokinetic power, both ultrasound muscle thickness and
284 appendicular or regional lean tissue provided similar correlation coefficients (excluding posterior

285 upper leg), indicating both metrics may be useful for the characterization of sarcopenia in older
286 males. In line with our findings, Thiebaud et al., 2017 observed similar correlations between 1
287 repetition maximum knee extension and flexion strength with either anterior to posterior thigh
288 muscle thickness ratio ($r= 0.39$ to 0.52) or appendicular lean tissue mass ($r= 0.46$ to 0.56).
289 Furthermore, the anterior to posterior upper arm muscle thickness ratio and appendicular lean
290 tissue mass displayed similar associations with 1 repetition maximum for chest press ($r= 0.54$
291 and $r= 0.65$, respectively) and lat-pull down ($r= 0.41$ and $r= 0.56$, respectively) (Thiebaud et al.
292 2017). However, these associations were evaluated across young, middle-aged, and older males;
293 whereas our study only focused on older males. In a more direct comparison, Tsukasaki et al.,
294 2020 examined quadriceps cross-sectional area (using computed tomography) and DXA lean
295 tissue mass in relation to isometric knee extensors torque in 1818 adults (40-89 years of age).
296 Although quadriceps cross-sectional area provided statistically stronger associations with muscle
297 strength than DXA appendicular or thigh lean tissue, the correlation coefficients were of similar
298 magnitude (males – cross-sectional area: 0.50 , DXA: 0.46 ; females – cross-sectional area: 0.49 ,
299 DXA: 0.40) (Tsukasaki et al. 2020). These data indicate that ultrasound is a clinically relevant
300 alternative tool to evaluate muscle size and draw inferences in relation to skeletal muscle
301 strength and power, providing an alternative tool to DXA for assessment of sarcopenia in older
302 adults. Furthermore, these data highlight that site-specific muscle size may provide an earlier
303 marker for identifying low skeletal muscle mass in older adults.

304 A potential advantage that ultrasound provides over DXA appendicular lean tissue in the
305 assessment of sarcopenia, is the ability to quantify a surrogate of muscle composition (echo
306 intensity) in addition to muscle thickness, which may provide complementary metrics for
307 evaluating ageing-related muscle degradation. While we observed that echo intensity was

308 correlated with isometric torque and isokinetic power, when both echo intensity and muscle
309 thickness were included as covariates in multiple linear regression, echo intensity was not
310 independently associated with muscle strength and did not improve the coefficient of
311 determination in comparison to muscle thickness alone. However, Watanabe et al., 2013
312 observed that both muscle thickness and echo intensity of the rectus femoris were significantly
313 associated with maximal isometric knee extensor torque in multiple-linear regression (B-
314 coefficients 0.381 and -0.294). These discrepancies are potentially due to the moderate
315 associations between muscle thickness and echo intensity in our cohort, whereas Watanabe et al.,
316 2013 did not observe any correlation. However, others have also observed inverse associations
317 ($r = -0.59$) between muscle thickness and echo intensity (Varanoske et al. 2020). This discrepancy
318 between our findings and those of Watanabe et al., 2013 is somewhat surprising given that we
319 recruited males of a similar age range (~65-90 years), but may potentially be due to differences
320 in ethnicity (Japanese vs. Caucasian) or ultrasound imaging protocol (e.g. standing vs. supine).
321 However, data from the Healthy Ageing and Body Composition study demonstrated that mid-
322 thigh cross-sectional area explained a much larger proportion of the variance ($R^2 = 0.304$ men
323 and $R^2 = 0.248$ women) in isometric knee extension torque than thigh muscle intramuscular
324 adipose tissue ($R^2 = 0.016$ men and $R^2 = 0.030$ women) (Goodpaster et al. 2001). These data
325 agree with our findings, suggesting that the majority of the variance in muscle strength is
326 explained by metrics of muscle mass (thickness, cross-sectional area), rather than composition
327 (echo intensity).

328 In relation to physical function, after correcting for multiple comparisons, neither DXA
329 nor ultrasound characteristics of muscle were associated with the six-minute walk or 30-second
330 sit to stand test; however, rectus abdominis echo intensity displayed moderate ($r = -0.47$)

331 associations with 30-second sit to stand. Others have observed that the ratio between the anterior
332 and posterior thigh muscle thickness is associated with zig-zag walking time, but not gait speed
333 (Abe et al. 2014b). Marcus et al., 2012 observed associations between six-minute walk distance
334 and thigh intramuscular adipose tissue ($r = -0.33$) and muscle cross-sectional area ($r = 0.38$) in 109
335 older adults. While we did not observe any association between function and thigh thickness or
336 echo intensity, the older adults Marcus et al., 2012 recruited were likely of poorer functional
337 capacity, as they had at least 2 comorbidities, were at risk of falling or had experienced a fall in
338 the past 12 months, and had a shorter six-minute walk distance (409.9 ± 120.3 compared with
339 540.9 ± 87.8 m).

340 An important limitation of this study is the lack of participants presenting with sarcopenia
341 (according to recent guidelines of low muscle strength and mass) (Cruz-Jentoft et al. 2018). In
342 our cohort, several participants presented with low appendicular lean tissue mass ($n=12$), but
343 only 2 had a low grip strength (<27 kg), which limit the generalizability of these findings to
344 individuals with sarcopenia. Furthermore, the individuals with low appendicular lean tissue were
345 significantly older (81.9 vs. 71.5 years) than those with normal appendicular lean tissue, making
346 it challenging to disentangle the effects of advancing age versus skeletal muscle atrophy for site-
347 specific comparisons of muscle thickness and lean tissue. In addition, our analyses only focused
348 on older males, which limiting our understanding of site-specific measures of skeletal muscle
349 mass and composition in relation to strength and function of older females.

350 **Conclusions**

351 In older males, site-specific measures of muscle thickness and DXA lean tissue provided
352 similar correlation coefficients with static and dynamic muscle strength. These data highlight
353 that both appendicular lean tissue and site-specific measures of muscle size (thickness, regional

354 lean tissue), are useful tools for assessing muscle mass in older adults for the identification of
355 sarcopenia.

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367

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510 **Table 1.** Participant characteristics

	All (n=32)	Low appendicular lean tissue (n=12)	Normal appendicular lean tissue (n=20)	Unadjusted p-value	Hedges' g (95% CI)
Age, y	75.4 (7.9)	81.9 (6.6)	71.5 (5.8)	<0.001	1.66 (0.84, 2.48)
Height, m	1.73 (0.08)	1.74 (0.07)	1.73 (0.08)	0.789	0.13 (-0.59, 0.84)
Body mass, kg	80.0 (13.3)	72.9 (8.2)	84.2 (14.1)	0.017	-0.90 (-1.65, -0.15)
BMI, kg/m ²	26.5 (4.0)	24.1 (1.8)	28.1 (4.3)	0.004	-1.09 (-1.85, -0.32)
Waist circumference, cm	99.3 (9.5)	95.5 (6.2)	101.5 (10.5)	0.079	-0.64 (-1.37, 0.09)
Appendicular lean tissue index, kg/m ²	7.28 (0.87)	6.48 (0.48)	7.76 (0.68)	<0.001	-2.03 (-2.90, -1.16)
Upper arm lean tissue, kg	1.65 (0.36)	1.36 (0.22)	1.76 (0.35)	0.001	-1.26 (-2.04, -0.48)
Lower arm lean tissue, kg	1.26 (0.19)	1.16 (0.17)	1.33 (0.17)	0.009	-0.97 (-1.73, -0.22)
Upper leg lean tissue, kg	5.50 (0.89)	4.90 (0.68)	5.86 (0.81)	0.002	-1.22 (-2.00, -0.45)
Lower leg lean tissue, kg	2.73 (0.38)	2.50 (0.34)	2.87 (0.34)	0.006	-1.06 (-1.82, -0.30)
Body fat, %	29.6 (4.2)	29.3 (3.3)	29.9 (4.7)	0.704	-0.14 (-0.85, 0.58)

511 Data are presented as mean (standard deviation [SD]). BMI, body mass index.

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516 **Table 2.** Strength and physical function characteristics

	All (n=32)	Low appendicular lean tissue (n=12)	Normal appendicular lean tissue (n=20)	Unadjusted p-value	Adjusted p-value	Hedges' g (95% CI)
Knee extensors isometric torque, Nm	168.5 (45.7)	141.9 (39.5)	184.5 (42.4)	0.008	0.048	-1.00 (-1.76, - 0.25)
Knee extensors 60 %/sec isokinetic power, W	138.6 (42.1)	113.7 (35.8)	153.6 (39.0)	0.007	0.049	-1.03 (-1.79, - 0.27)
Knee extensors 180 %/sec isokinetic power, W	288.8 (87.9)	243.4 (72.6)	316.0 (86.4)	0.021	0.105	-0.87 (-1.61, - 0.12)
Knee flexors isometric, Nm	88.6 (23.0)	72.5 (13.0)	98.3 (22.4)	0.001	0.009	-1.29 (-2.07, - 0.51)
Grip strength, kg	38.4 (8.9)	34.5 (8.7)	40.7 (8.4)	0.055	0.165	-0.71 (-1.45, 0.03)
Elbow extensors isometric torque, Nm	62.9 (17.1)	54.8 (14.5)	67.8 (17.1)	0.035	0.140	-0.78 (-1.52, - 0.04)
Elbow flexors isometric torque, Nm	51.2 (15.4)	40.3 (11.1)	57.7 (14.1)	0.001	0.008	-1.30 (-2.08, - 0.51)
Six-minute walk distance, m	540.9 (87.8)	519.1 (103.0)	554.1 (77.1)	0.282	0.282	-1.50 (-2.31, - 0.70)
30-second sit to stand, repetitions	15.3 (4.9)	13.6 (4.6)	16.3 (4.9)	0.155	0.310	-0.55 (-1.28, 0.18)

517 Data are presented as mean (SD). Adjusted p-values were derived using a Holm-Bonferroni correction.

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520 **Table 3.** Muscle thickness characteristics

	All (n=32)	Low appendicular lean tissue (n=12)	Normal appendicular lean tissue (n=20)	Unadjusted p-value	Adjusted p-value	Hedges' g (95% CI)
Anterior upper arm, cm	3.15 (0.50)	2.78 (0.28)	3.37 (0.47)	<0.001	0.002	-1.4 (-2.19, -0.61)
Posterior upper arm, cm	2.81 (0.74)	2.39 (0.52)	3.06 (0.75)	0.011	0.032	-0.97 (-1.72, -0.21)
Anterior forearm, cm	4.60 (0.50)	4.21 (0.45)	4.84 (0.38)	<0.001	0.002	-1.51 (-2.31, -0.7)
Anterior abdomen, cm	0.87 (0.19)	0.76 (0.18)	0.93 (0.17)	0.012	0.023	-0.95 (-1.71, -0.2)
Anterior upper leg, cm	2.68 (0.67)	2.26 (0.38)	2.94 (0.67)	0.003	0.007	-1.14 (-1.91, -0.37)
Posterior upper leg, cm	4.42 (0.92)	3.79 (0.85)	4.79 (0.76)	0.002	0.006	-1.23 (-2, -0.45)
Anterior lower leg, cm	2.97 (0.28)	3.06 (0.22)	2.82 (0.32)	0.021	0.021	0.81 (0.07, 1.56)
Posterior lower leg, cm	6.16 (0.79)	5.56 (0.71)	6.54 (0.58)	<0.001	0.001	-1.51 (-2.32, -0.71)

521 Data are presented as mean (SD). Adjusted p-values were derived using a Holm-Bonferroni correction.

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526 **Table 4.** Muscle echo intensity characteristics

	All (n=32)	Low appendicular lean tissue (n=12)	Normal appendicular lean tissue (n=20)	Unadjusted p-value	Adjusted p-value	Hedges' g (95% CI)
Anterior upper arm, AU	63.5 (11.9)	66.0 (11.8)	62.0 (12.0)	0.371	0.741	0.33 (-0.39, 1.05)
Posterior upper arm, AU	35.3 (9.7)	40.2 (10.9)	32.3 (7.8)	0.023	0.092	0.85 (0.10, 1.6)
Anterior abdomen, AU	58.4 (18.9)	67.5 (21.4)	53.0 (15.3)	0.034	0.101	0.79 (0.05, 1.54)
Anterior upper leg, AU	52.5 (13.9)	62.8 (11.4)	46.3 (11.6)	<0.001	0.003	1.40 (0.60, 2.19)
Anterior lower leg, AU	55.6 (12.2)	63.4 (10.7)	50.9 (10.6)	0.003	0.016	1.15 (0.38, 1.91)
Posterior lower leg, AU	80.1 (17.6)	81.4 (21.9)	79.4 (14.9)	0.761	0.761	0.11 (-0.61, 0.83)

527 Data are presented as mean (SD). Adjusted p-values were derived using a Holm-Bonferroni correction. AU,
 528 arbitrary units.

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533 **Table 5.** Correlation coefficients between muscle thickness, muscle echo intensity, appendicular lean
 534 tissue index, or region-specific lean tissue and maximal muscle torque or power.

	Muscle thickness	Echo intensity	Appendicular lean tissue index	Region-specific lean tissue
Knee extensors isometric torque, Nm	0.5 (0.18, 0.72)	-0.41 (-0.66, -0.07)	0.52 (0.20, 0.73)	0.70 (0.46, 0.84)
Knee extensors 60 °/sec isokinetic power, W	0.55 (0.24, 0.75)	-0.47 (-0.70, -0.14)	0.57 (0.27, 0.76)	0.71 (0.48, 0.84)
Knee extensors 180 °/sec isokinetic power, W	0.62 (0.34, 0.79)	-0.48 (-0.70, -0.15)	0.57 (0.27, 0.76)	0.63 (0.36, 0.80)
Knee flexors isometric, Nm	0.39 (0.04, 0.65)	-	0.69 (0.44, 0.83)	0.71* (0.48, 0.84)
Grip strength, kg	0.53 (0.22, 0.74)	-	0.63 (0.36, 0.80)	0.65 (0.38, 0.81)
Elbow extensors isometric torque, Nm	0.71 (0.48, 0.84)	-0.59 (-0.77, -0.30)	0.66 (0.40, 0.82)	0.83 (0.67, 0.91)
Elbow flexors isometric torque, Nm	0.58 (0.28, 0.77)	-0.43 (-0.67, -0.09)	0.58 (0.28, 0.77)	0.65 (0.38, 0.81)

535 Data are presented are correlation coefficient (95% CI). Bold value indicates significant correlation after Holm-
 536 Bonferroni correction. * indicates a significantly different correlation coefficient between regional lean tissue or
 537 muscle thickness in relation to isometric torque or isokinetic power. Correlation coefficients for muscle thickness
 538 and echo intensity were derived between: anterior upper leg and knee extensors (torque and power), posterior upper
 539 leg and knee flexors (torque), anterior forearm and grip strength, posterior upper arm and elbow extensors (torque),
 540 anterior upper arm and elbow flexors (torque). Correlation coefficients for regional lean tissue were derived
 541 between: upper leg lean tissue and knee extensors (torque and power) and flexors (torque), lower arm lean tissue and
 542 grip strength, upper arm lean tissue and elbow extensors (torque) and flexors (torque).

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547 **Table 6.** Multiple linear regression analysis of muscle thickness and echo intensity compared to maximal
 548 muscle torque or power.

	Muscle thickness standardized B coefficient	Muscle thickness p-value	Echo intensity coefficient	Echo intensity p-value	Regression coefficient
Knee extensors isometric torque, Nm	0.395	0.06	-0.158	0.45	0.51
Knee extensors 60 °/sec isokinetic power, W	0.420	0.04	-0.203	0.31	0.57
Knee extensors 180 °/sec isokinetic power, W	0.531	0.009	-0.136	0.47	0.63
Elbow extensors isometric torque, Nm	0.566	0.002	-0.231	0.16	0.73
Elbow flexors isometric torque, Nm	0.488	0.006	-0.204	0.23	0.61

549 Data are presented as standardized B-coefficients. Regressions for muscle thickness and echo intensity were derived
 550 between: anterior upper leg and knee extensors (torque and power), posterior upper arm and elbow extensors
 551 (torque), anterior upper arm and elbow flexors (torque).

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556 **Table 7.** Correlation coefficients between muscle thickness, muscle echo intensity, appendicular lean
 557 tissue index, or region-specific lean tissue and six-minute walk distance or 30-second sit to stand.

		six-minute walk	30-second sit to stand
Anterior abdominal	thickness, cm	0.12 (-0.23, 0.44)	0.09 (-0.26, 0.42)
	echo intensity, AU	-0.30 (-0.58, 0.05)	-0.47 (-0.70, -0.14)
Anterior upper leg	thickness, cm	0.04 (-0.31, 0.38)	0.1 (-0.25, 0.43)
	echo intensity, AU	-0.17 (-0.48, 0.19)	-0.11 (-0.44, 0.24)
Posterior lower leg	thickness, cm	0.25 (-0.10, 0.55)	-0.06 (-0.40, 0.29)
	echo intensity, AU	-0.03 (-0.37, 0.32)	-0.25 (-0.55, 0.10)
Lean tissue	Appendicular lean tissue index, kg/m ²	0.12 (-0.23, 0.44)	0.03 (-0.32, 0.37)
	Lower body lean tissue, kg	0.29 (-0.06, 0.58)	-0.05 (-0.39, 0.30)

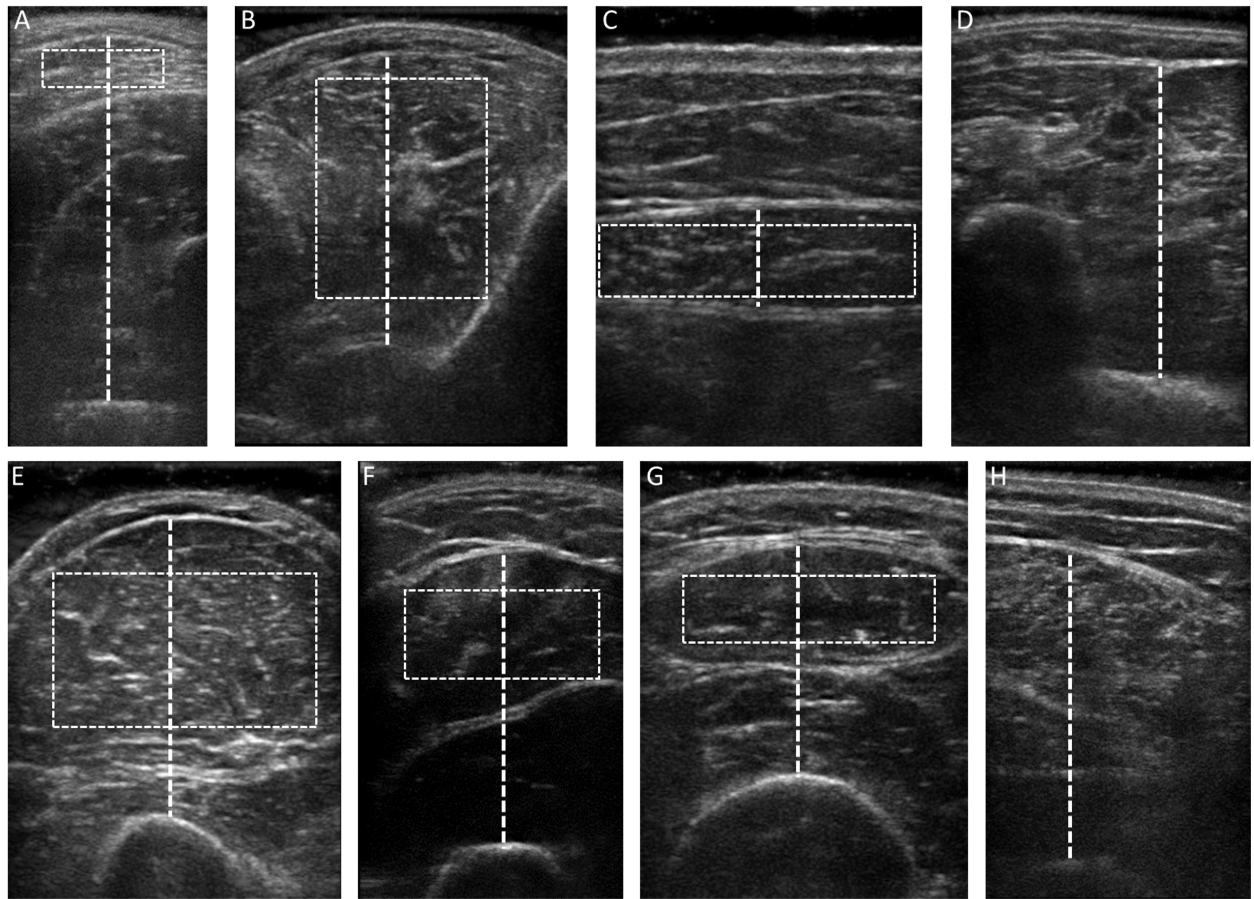
558 Data are presented are correlation coefficient (95% CI). Bold value indicates significant correlation after Holm-
 559 Bonferroni correction. AU, arbitrary units.

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563 **Figure 1**



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572 **Figure captions**

573 Figure 1. Representative ultrasound images for analysis of skeletal muscle thickness and echo
574 intensity of the A) posterior lower leg, B) anterior lower leg, C) anterior abdominal, D) anterior
575 forearm, E) anterior upper arm, F) posterior upper arm, G) anterior upper leg, H) posterior upper
576 leg.